

Review: Sustained Release and Formulation Strategies for Nifedipine

Pandurang Sanjay Sawant

B.R Harne college of Pharmacy (vangani)

Department of Pharmaceutics, University of Mumbai

Abstract—Because the medication does not reach the site of action in the proper amounts, conventional drug delivery methods for treating hypertension and angina are not very effective. Strong and cautious treatment for angina and high blood pressure disorder using a certain medicine delivery method is difficult for the pharmaceutical experts. The most popular approach to drug regulation release is to incorporate it into a matrix system due to its hydrophilic and pliable nature. In oral controlled medication administration, polymer matrices are frequently utilized to achieve a systematic, wide-ranging regulatory compliance, and a desired medication release pattern. Nifedipine sustained release matrix tablet formulation was created by The polymers combine to produce the desired profile of medication release. Evaluation The prepared pills' hardness, friability, thickness, and medication content homogeneity, weight fluctuation, and the pattern of in vitro drug release. 97% of the drug was released at 24 hours in the formulation made with HPMC K100M, while 99% of the drug was released at 20 hours in the formulation made with Eudragit. The current study's goal was to create and assess a sustained release matrix tablet of nifedipine using natural polymers. The tablets were made using direct compression technique utilizing various Guar dosages gum and Xanthan gum as organic polymers. The ready Tablets were assessed for pre-compression characteristics such bulk density, angle of repose, tapped density, Hausner's ratio, compressibility index, and post-compression factors like thickness, hardness, and weight fluctuation, friability, consistency of substance, swelling index, and in vitro studies on disintegration. FTIR analysis revealed that there was no drug-polymer interaction. The best possible sustained Drug release over a 12-hour period was demonstrated by formulation F9. The improved formulation's "n" value showed that the medication release adheres to the unusual non-Fickian Release The stability investigations verified that the optimized formulation held steady at 40 °C and 75% relative humidity.

Keywords—Nifedipine, Control release, GITS, Matrix Tablets, Pharmacokinetics, Zero-order Release, Hypertension.

A modified dose form known as a sustained release dosage form extends the medication's therapeutic action.[1,2] Products with sustained release offer an instantaneous release of medication that quickly creates the intended therapeutic impact, which is followed by a slow release of further doses of medication to maintain this effect over a set amount of time. [5] Products with continuous release frequently periods makes it unnecessary to take medication at night, which has advantages for the patients as well as the treatment provided due to the ongoing drug levels in plasma [1,2]. A continuous medication delivery system's primary goal is to maximize A drug's pharmacodynamic and pharmacokinetic characteristics in a manner that maximizes its usefulness by minimizing side consequences and treatment or management of the ailment through the most efficient method of administering the least amount of medication.[6] The oral route has been the most well-liked and extensively utilized for long-term medication delivery due to its ease and more adaptability in dosage form formulation, simplicity of administration, Low cost and ease of manufacture The majority of traditional oral medication preparations, such tablets and capsules, are designed to release the active ingredient right away following oral administration in order to provide quick and total absorption of the medication throughout the body. Such instantaneous Drug absorption and onset are accelerated by release products. of action. Drug concentration in plasma decreases in accordance with to the pharmacokinetic characteristics of the medication upon absorption of The medication is fully included in the dose form. Drug concentrations in plasma drop below the minimum effective plasma concentration (MEC), which leads to the inability of effectiveness of treatment. Prior to reaching this moment, the other is typically used if a long-lasting therapeutic result is desired. The alternative method of giving a dosage is by using a dosing form that will provide the medication a prolonged release by

I. INTRODUCTION

preserving the drug concentrations in plasma [3, 4] The yellow, crystalline drug nifedipine (NF) is soluble in ethanol but nearly insoluble in water. NF is a specific calcium-channel inhibitor and peripheral arterial vasodilator that directly affects smooth muscle in the arteries. NF is frequently utilized in the therapy for systemic angina pectoris hypertension.[8] The medication is weakly soluble, and its The gastrointestinal tract's absorption is restricted by rate of disintegration. Its biological half-life is brief (4 hrs). NF absorption is minimal after oral delivery using an immediate-release dosage forms. It has an oral bioavailability of 45–65% [9] because first-pass metabolism in the liver. instantaneous release NF formulations clearly demonstrate drug variation. Certain adverse effects are caused by plasma concentration. such as a rise in heart rate. Sublingual NF has been utilized in situations with hypertension, found to be unsafe form Drug delivery methods known as sustained release formulations are made to constantly release drugs in order to increase their therapeutic efficacy. for a long time following administration of one dosage. To lessen the occurrence of administration and to enhance patient adherence, a once NF's daily sustained-release formulation is desirable. The most popular technique for controlling Drug release occurs when a drug is incorporated into a matrix. system. The tablet with a direct compressed matrix has been utilized for many years because of its affordability and ease of use. Comparing efficiency with alternative medication delivery methods systems [2, 11,12]. Hydrophilic polymers are extensively utilized in matrix systems. The hydrophilic HPMC polymer utilized in the creation of oral controlled medication delivery systems as a carrier that delays release.

The primary objectives of Nifedipine SR formulation are:

percentage of polymers utilized in the preparations. Researchers have focused more on the advancement of continuous release or because of the intricacy and cost associated with the promotion of novel pharmaceutical products The formulation for sustained release is those which provide a long-lasting, gradual action. For example, providing action for an extended length of time without impairing the concentration of the medication. Sustained release formulation keeps the medication plasma consistent. concentration. However, all kinds of medications cannot be given using the prolonged release the medication. tablet with an enteric coating and

Implantable tablets and capsules are examples of this. kind of system. The mechanism of the reservoir type is connected to this kind of system. Extended action Improvement of the drug's half-life Slow motion Low rate of dissolution Site-specific action Enteric-coated materials and Hardness of tablets Both synthetic and natural polymers [1,2]

II. MATERIAL

Anode supplied nifedipine Pharma, Kanpur, H.P.M.C. K 100, Ethyl Cellulose, Talc, magnesium stearate SD, and H.P.M.C. K 4 by Merck Limited (India) Drug, polymer, and excipient fine chemical quantities that are required and securely put into polyethylene bag, and the mixture was combined for at least 15 min. After that, the mixture was lubricated. by mixing once more after adding 1% magnesium stearate. for a further five minutes. Sustained Release Formulation Strategies [2]

Matrix System Types

Depending on the kinds of polymeric materials or retarding agents, the matrix system can be split into two groups.

- 1) Hydrophobic matrix structure
- 2) A system of hydrophilic matrice matrix system that is hydrophobic.

This is the only technique that does not require the use of polymers in order to produce controlled substances. release, despite the usage of insoluble polymers. The primary rate, as the name implies, The hydrophobic matrix's governing elements are naturally insoluble in water. These Waxes, glycerides, fatty acids, and polymeric substances like ethyl cellulose, acrylate copolymer, and methyl cellulose. To control the release of drugs, it could be Lactose and other soluble substances must be included in the formulation. During drug release, the formulations' insoluble component aids in preserving the hydrophobic matrix's physical dimensions. Therefore, the active ingredient's dispersion from the The release mechanism is the system, and the associated release characteristic can be defined by the square root of time release kinetic, a Higuchi equation. With a porous monolith, the square root of time release profile is anticipated, where the release is proportionate to the drug loading from such a system. Furthermore, a hydrophobic matrix Systems are typically unsuitable for drugs that are insoluble because the concentration gradient is too low to provide sufficient medication release. Therefore,

based on the real characteristics of the ingredient or formulation design, insufficient medication release in The duration of the gastrointestinal transit is a possible danger and must be identified when the project is being developed. Given the increasing need for therapeutic optimization, matrix systems with configurable delivery rates have grown in significance. One of the main goals of constant rate delivery has always been regulated release method, particularly for medications having a limited therapeutic index. matrix system that is hydrophilic Polymers that would swell are the main components of a hydrophilic matrix that limit rate. when they come into contact with an aqueous solution and create a gel layer on the system's surface. When a polymer and the releasing medium, such as water, are thermodynamically compatible, the solvent enters the voids that exist between macromolecular chains. The polymer could go through a relaxing process because of the strain of the pierced the solvent, allowing the polymer The matrix expands and the chains become more pliable. This enables the medication that is encapsulated to diffuse out of the matrix more quickly. However, it would take longer for the medication to diffuse out of the matrix because the diffusion channel is lengthened by matrix swelling. It has been It is well recognized that there are other elements besides swelling and diffusion that affect the pace of drug discharge. Polymer dissolution is another crucial mechanism for dissolvable polymer matrices that might adjust the rate at which drugs are delivered. Although swelling or disintegration may be the most common factor for a particular kind of polymer, drug release kinetics are typically caused by a mix of these two processes.[1,9]

2. Osmotic Pump Systems (GITS)

Basic Osmotic Pump System Components 2.1. Drug Not all drugs that are provided must have a long-lasting effect, thus the osmotic Not every medication can be used with a pump device. Medications that are recommended for the extended The greatest candidates for therapy of illnesses with biological half-lives between one and six hours include osmotic systems. Medications with a biological half-life of less than an hour are not suitable options. Additionally, medications with a half-life longer than 12 hours are not suitable for regulated release within an osmotic pump system. The medication should have a brief half-life so that it can be kept in plasma, and that its extended release ought to be the necessity . In order to be included in this

system, medications should also be neither either extremely soluble or extremely weakly soluble, and the drug's nature should be strong for this intent [1,9,13].

2.2. The Osmotic Agent

Osmotic agents are sometimes known as osmogens or osmogents, and they produce the osmotic delivery system's osmotic pressure. A medication with poor solubility will be released at a slow, first-order rate; osmotic drugs are employed to increase this pace within the formulation. These substances produce a significant osmotic pressure gradient inside the osmotic mechanism; thus, the drug release rate rises . The available osmotic agents Lactose, fructose, sorbitol, dextrose, sodium chloride, and citric acid are among the products available. Pharmaceuticals 2022, 15, 1430, 4 of 16 mannitol, xylitol, sucrose, and potassium chloride. Additionally, osmogens may comprise blends, such as sucrose + fructose, mannitol + sucrose, dextrose + sucrose, mannitol plus fructose, lactose plus fructose, mannitol plus dextrose, or lactose plus dextrose . Osmotic agents include medications like mannitol, glycerol, and others that are soluble in water. polyethylene glycol, sorbitol, or lactulose. But osmogenic salts, such sodium chloride ,and potassium chloride), as well as carbohydrates, can be added to the medication's formulation if has little osmogenic activity on its own. [9,13]

Observation: Drug release research in vitro

Dissolution apparatus type 2 (USP XXVIII) in 900 ml of sodium phosphate was used for in vitro release rate investigations. buffer (pH 7.4) containing 1% w/v sodium lauryl sulfate at $37 \pm 0.5^\circ\text{C}$. 50 rpm was used as the stirring speed. At A 5-ml sample was taken out at prearranged intervals. then changed out for up to 12 hours with new dissolving material. After The samples were examined using the UV at the proper dilutions. spectrophotometric technique at 238 nm. Total percentage of medication released was computed, and the average of three tablets Data analysis was done using each of the three batches. Release kinetics characterization To investigate nifedipine's release kinetics from the matrix tablets, the release information was fitted to the following

equations: Equation of zero order $Q.t = k_0$ where Q is the proportion of drugs released at a given time. K_0 and t is the rate of release constant; Equation of first order [1]

$\ln(100-Q_t) = \ln 100 - k_1 t$
 where k_1 is the rate of release constant; Higuchi's formula [24] $Q_t = k_H \cdot t^{1/2}$, where k_H is the constant for the Higuchi release rate; Additionally, to more accurately describe the medication release mechanisms for the polymeric systems under investigation, Korsmeyer The semi-empirical model of Peppas [25] was used: $Q_t / Q_\infty = k K P \cdot t^n$. The percentage of drug released is Q_t / Q_∞ . $k K P$ is a constant at time t that jeopardizes the structural and geometric properties of the apparatus, and n , the release exponent, which represents the drug's mechanism release. When it comes to cylindrical shapes like tablets, A Fickian diffusion release (Case I) is represented by $n=0.45$. $0.45 < n < 0.89$ to an anomalous (non-Fickian) transport, $n = n > 0.89$ to zero order (Case II) release kinetics and 0.89 to A super Case II transport. In order to fit the release data to the calculations, only the points between 10% and 70% were used. The range for the Higuchi model was 10–60%. [1]

Dissolution Temperature: 37 0.5°C; medium volume: 900 mL Basket paddle speed: 50 rpm Sampling intervals: 10 and 30 minutes Sample removal: 5 mL Measured absorbance: 237 nm, 235 nm DRUG RELEASE ANALYSIS The data from conducted research was fitted into zero order, first order, Higuchi matrix, and Korsmeyer-Peppas constant to analyze the mechanism for the release and release rate kinetics of the manufactured dosage form. In this case, the best-fit model was chosen by comparing the derived r-values. [1,15]

Kinetics of Zero Order

The following equation can be used to describe drug dissolution from pharmaceutical dosage forms that do not disintegrate and release the medication gradually, provided that the area remains unchanged and no equilibrium conditions are reached. $Q_0 + K_0 t = Q_t$ where Q_0 is the starting drug concentration in the solution and Q_t is the amount of medication dissolved in time t . K_0 stands for zero order release. Details of Vitro DRUG Release Studies Tools

utilized: Dissolution test apparatus USP XXIII
 Dissolution medium: 6.8 pH phosphate and 1.2 pH acidic [15]

Kinetics of the First Order

The release rate data were fitted to the following equation in order to examine the first order release rate kinetics. $\log Q_t = \log Q_0 + K_1 t / 2.303$ where K_1 is the first order release rate constant, Q_t is the amount of drug released in time t , and Q_0 is the starting amount of drug in the solution. HIGUCHI MODEL To investigate the release of water-soluble and low-soluble medications in corporate semisolids and/or solid matrices, Higuchi created a number of theoretical models. For drug particles distributed in a uniform matrix acting as the diffusion media, mathematical formulas were found. $Q_t = K H \cdot t^{1/2}$ where $K H$ is the Higuchi dissolving constant and Q_t is the amount of medication released in time t . PEPPAS AND KROSMEYER RELEASE MODEL The following equation is fitted to the release rate data in order to examine this model. K is the release constant, t is the release duration, n is the diffusional exponent for the drug release that depends on the slope of the matrix dosage forms, and M_t / M_∞ is the fraction of drug release. [15]

III. STABILITY STUDIES

The ability of a medication formulation to stay within its physical, chemical, therapeutic, and toxicological requirements in a particular container is known as stability. Stability testing is used to establish recommended storage conditions, retest periods, and shelf lives by demonstrating how the quality of a drug substance or drug product changes over time under the influence of various environmental factors like temperature, humidity, and light. ICH DEFINES STUDY LENGTH AND STORAGE CONDITIONS 30 days of accelerated testing at 40°C ± 20°C and 75% RH. Stability tests for the chosen formulation were conducted in the current study at 40°C and 75% relative humidity for a duration of up to 30 days. [15]

Table 1: In vitro drug dissolution studies

TIME (H)	IR TABLET (% RELEASE + SD)	SR MATRIX TABLET (%RELEASE + SD)	SR GITS TABLET (%RELEASE ± SD)
0.5	64.2 ± 3.4	16.5 ± 1.4	5.4 ± 0.6
4	96.7 ± 5.2	49.9 ± 2.6	28.2 ± 1.6
8	-	70.1 ± 3.8	50.7 ± 2.4
12	-	88.0 ± 4.2	72.2 ± 3.8

24	-	92.1 ± 5.4	95.8 ± 4.4
Release Kinetics	First-Order	Higuchi Model	Zero order

Percentage release drug ± Standard moment.

Diagram: Drug Release Kinetics Comparison

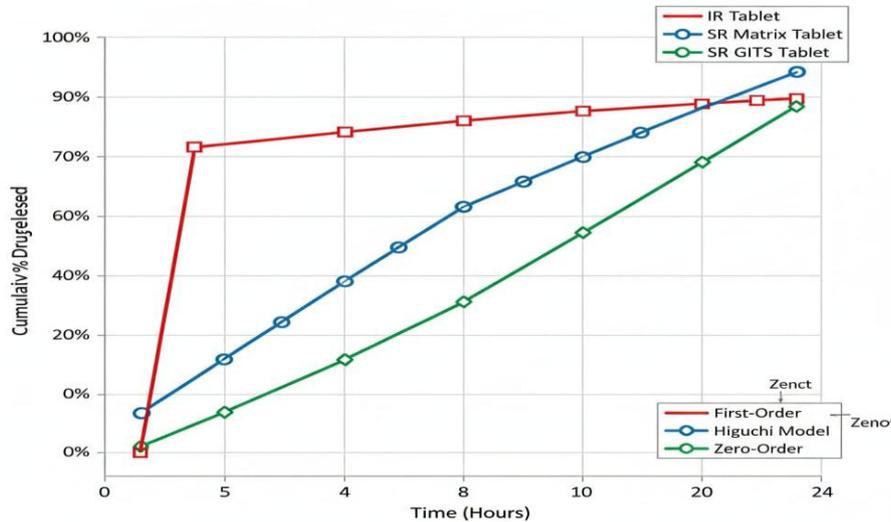


Figure 1: Comparative *In Vitro* Drug Release Profiles of Nifedipine Formulations, highlighting the shift from rapid first-order-release (GITS).

This diagram achieve therapeutic drug concentration .[1,3,,15]

Evaluation of Drug

1. Diameter and Thickness

The tablets' dimensions and thickness were determined with a Vernier calliper. Five tablets were utilized from each batch, and the average Values were computed.[11]

2. Test of Weight Variation

Twenty pills of each were used to examine weight variation. formulation were measured with an electronic balance (Shimadzu's AW-220), and the test was completed in accordance with the official method.[11]

3. The presence of drugs

Each of the five tablets was weighed separately and triturated. The average amount of powderThe tablet's weight was measured, and the medicationwas removed for six hours in water. The A 0.45µ membrane was used to filter the fluid.At 226.5 nm, the absorbance was measured. following an appropriate dilution.[11]

4. Hardness

The hardness of six pills for each formulationwere calculated using the Monsanto hardness tester (Cadmach). The tablet was held between the tester's two jaws along its oblong axis. The reading should be

0 at this moment. kg/cm2Next, a steady force was delivered by turning the knob till the tablet broke. The value was recorded in kg/cm at this point.2 Typically, at least 4 kg/cm2 Hardness is regarded as suitable for tablets without coating. [11]

5. Friability

The friability of six pills for each formulation were ascertained with the Roche friabilator (Lab Hospital). This test involves a variety of tablets to the combined impact of shock abrasion with the use of a plastic chamber that rotates at 25 revolutions every minute, lowering the tablets with a 6-inch gap between each revolution. An example of preweighed

The Roche friabilator was filled with U6 tablets and run for 100 revolutions, or four minutes. The After that, the tablets were powdered and weighed again. A reduction in weight of less than 1% in general regarded as appropriate 49

Friability percentage (%)

F) was computed as follows:

$$\%F = \frac{W - W_0}{W_0} \times 100 \quad [11]$$

6. Studies on In Vitro Release

Drug release investigation in vitro for the prepared Matrix pills were used for eight hours using a USP XXVI type II six-station (paddle) device at 50 rpm and 37°C ± 0.5°C speed. The investigations on dissolving were conducted. for eight hours in triplicate in phosphate buffer of pH 6.8 under sink

conditions. For the first thirty minutes and then 5 ml samples per hour were taken out of the dissolving solvent and swapped out with new medium to keep the volume steady. Following filtering and suitable dilution, the sample solution was tested for nifedipine HCl at 226.5 nm using a UV spectrophotometer. The dosages of medication found in the samples were computed using the with the use of a suitable calibration curve built from reference standard

7. Polymer swelling or water uptake investigations

The rate at which the test media is absorbed by the equilibrium was used to determine the polymer. way of gaining weight. The investigation was conducted within the USP/NF dissolving apparatus [46,46] I. Polymer matrices were precisely weighed. put in containers for dissolving, submerged in 0.05M pH 6.8 phosphate buffer and kept the dissolving temperature at $37 \pm 0.5^\circ\text{C}$. vessels. Regularly, the pre-weighed The basket-matrix system was removed from the disintegration vessel, very lightly After removing extra test liquid with tissue paper, the weight was recalculated. The percentage of water absorption, or the amount of swelling brought on by the test liquid absorbed, was calculated at every time interval using the the following formula: percentage of water absorption or polymer swelling = $(W_s - W_i) \times 100$

W where W_s represents the swelling matrix at time t , W_i The starting weight of the matrix, and W_p represents the weight of the polymer within the matrix. [3,11,15]

8. Studies on matrix erosion

The typical USP/NF dissolving device I was employed in this way. After being weighed, the dried matrices were put in dissolution baskets, and exposed to dissolving in 500 milliliters of 0.05M phosphate buffer (pH 6.8) kept at $37 \pm 0.5^\circ\text{C}$ with the baskets spinning at 100 revolutions each minute. At regular intervals, basket-matrix assemblies were taken out of the dissolving containers and dried at 50°C in a hot air oven until the weight remained consistent. The matrix erosion percentage at The following was used to estimate time t . equation: Matrix erosion (%) = $(W_i - W_t) \times 100$

W_i

Where

W_i is the matrix's initial weight, W_t Is the matrix's weight vulnerable to erosion? during the duration t . [3,11,15]

IV. ADVANTAGE

The Extended Release Delivery System has advantages. Drug dose frequency is decreased with extended release formulations. Extended release formulations have the potential to sustain therapeutic concentrations. Reduce the toxicity by delaying the absorption of the medication. By using these formulations, the excessive blood concentration is avoided. Formulations with extended release have the potential to enhance patient compliance and convenience. Reduce both systemic and local adverse effects. Protect the medicine from hydrolysis and other degradative processes to increase its stability. throughout the digestive system. An increase in the effectiveness of treatment. Reduce drug buildup by using long-term dosage. Boost some medications' bioavailability. Use of fewer drugs overall. Enhance the capacity to deliver extraordinary effects. For instance, using bedtime medication to relieve arthritis in the morning. [1,9]

V. DISADVANTAGE

The extended release delivery system has drawbacks. [4] Because the drug dose in extended release formulations is larger, any loss of integrity of the dose form's releasing properties. Extended release products may be more difficult to swallow or transport due to their bigger size. via the stomach. A number of factors, including food and transit speed, have an impact on the release rates. via the stomach. There are variations in the rate of release between doses, however these have been reduced by contemporary formulations. Preparation is expensive. Occasionally, the target tissue will be exposed to a consistent dosage of medication over a lengthy period of time. Drug tolerance develops during this time. [1,9,16]

VI. LIMITATIONS AND PROSPECTS FOR THE FUTURE

This study offers a thorough summary of the pharmacologic treatment of critical hypertension, emphasizing the special advantages of the sustained-release formulation of nifedipine. Although worldwide statistics have been incorporated, Regional differences in the prevalence of hypertension. Although therapy outcomes might not be completely-tured, which might have an impact on the applicability of specific conclusions to particular

demographics with vital hypertension. Furthermore, the quick The development of medicines for hypertension implies because new advancements in therapy and New long-term efficacy information will keep coming in. enhance upcoming insights. [16]

VII. RESULT & DISCUSSION

Long-acting nifedipine formulations, like GITS, have shown advantages that go beyond basic hypertension treatment. successfully dealing with uncontrollable and resistant hypertension in addition to ailments like exertional angina, ischemia illness, and chronic Diabetes, renal insufficiency, and kidney disease Future studies could investigate these benefits by looking at the long-term results of nifedipine with continuous release in di-verse patient groups and looking into new combinations of therapies that include new antihypertensive medications. Such a study This could aid in improving clinical strategies, improve patients' quality of life and address the burden of hypertension worldwide. Effectively Nine formulations with varying polymer concentrations (HPMC-K100, HPMC-K4) were made directly compression technique and assessed for buoyancy lag time, physicochemical characteristics, overall floating time as well as medication release in vitro. The findings showed that optimum formulation N 6 on immersion in a pH 1.2 and 6.8 0.1N HCl solution Tablets with pH phosphate buffer at $37 \pm 0.50^\circ\text{C}$ as soon as possible and stay buoyant for 12 hours. without breaking down. The two primary elements are necessary for the tablet to gain bulk density.

1, just because it will continue to float on the stomach fluid. The optimum medication release data formulation following in vitro tests was exposed to Fit test positivity using linear regression analysis In accordance with the first order, zero order kinetic equation, Higuchi's and Korsmeyer's models to ascertain the medication release mechanism. When The values of the regression coefficient were compared, It was noted that "r" values of Higuchi was at its highest, or 0.978, thus showing that the drug's release from formulations was discovered to adhere to Higuchi kinetics. We are considering creating a matrix medication. medication delivery system only as a result of recent technological advancement. In the current study matrix Nifedipine tablets were made and assessed. This tablet has an API layer called layer of the matrix. This tablet might be useful in lowering Multiple dosage therapy for people with depression

have trouble taking many doses of the medication. An appropriate analytical technique based on A UV visible spectrophotometer was created. for nifedipine. A λ max of 276 nm was used to determine HCL remedy. Using the FT-IR First, all formulations' before and post compression parameters for the powder mix, such as bulk density, tap density, Carr's index, Hausner's angle of repose and ratio. that value fell inside the acceptable range. for Every formulation was represented by every evaluative criteria, such as weight fluctuation thickness, friability, hardness, and drug content [2 ,11]

VIII. CONCLUSION

Data from the in vitro assessment of the Nifedipine matrix tablet showed a lengthy medication release through various formulation factors Tablets with various release kinetics may be acquired. so that the steady release of nifedipine Tablets are the best medication for the antihypertensive individual. Considering all of these Considerations led to the discovery of formulation number N6. to be an optimal formulation, all of the outcomes of table demonstrates that the outcome was that all the The Matrix Tablet's specifications were discovered to be adequate for the intended usage. In terms of pharmacology, bioavailability is a gauge of the speed and degree to which a medication arrives at the action location. It is indicated by the letter F (or, if stated in if stated as a percentage,) in other Therefore, bioavailability might be defined as the rate and amount of medication that enters the systemic circulation of a drug or another substance percentage that goes into the systemic circulation when the medication entered the body, which is why It can have an active effect. In the N6 formulation, the proportion of Among all formulations, HPMC K100 is higher. Once every assessment parameter has been finished, it is discovered that this formulation's bioavailability is greater than everything else. In order for us to state that if the HPMC 100 is used in the NIFEDIPINE Tablet. 62.5% of the preparation formula. The tablet's bioavailability is rising. Additionally, it boosts efficacy and may be helpful in lowering the frequency of administration. The highly efficient and typically well Calcium is a well-tolerated antihypertensive medication. blockage of channels. are advantages of the calcium channel blockers have a prolonged duration of action. and a positive profile of adverse effects, and they are mostly recommended for patients. 30% to 40% of

Individuals with high blood pressure are given a calcium channel blocker in research that is observational, The prevalence of their use is rising. Drug disposition and bioavailability separated based on body weight and body weight loss during bariatric surgery. This research assessing the impact of body weight and body weight decrease on the pharmacokinetics of various drug users, and their outcomes are contrasted in to the three patient groups getting either a gall bladder surgery, gastric bypass, or a calorie diet at a very low level. HPMC K100 gum usage was extremely efficient in achieving the long-term medication release for 12 hours after taking sustained-release nifedipine pills. It was discovered that the drug release kinetics were described using a zero-order equation. The outcome of anomalous diffusion was that the releasing method. Erosion and diffusion drug release mechanism Both are connected. from the matrix-shaped tablets were determined using SEM research. Choosing a polymer Concentration and mixture were crucial. in delaying matrix tablet effectiveness. The medication As the number of tablets increases, the release rate drops. which is contained in a matrix form was also looked at, and it Based on the current study, it was determined that sustained released profile is kept up to date for an long durations with a safety margin

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