

# Latest Technology in Sensors Used for H<sub>2</sub>O<sub>2</sub> Detection

Asif Ali Khan<sup>1</sup>, Dr. Zulkharnain Mohammed<sup>2</sup>, Mohammed Rizwan Shaik<sup>3</sup>

<sup>1,3</sup>College of Engineering and Computer science, Jazan University, Saudi Arabia

<sup>2</sup>College of Applied Industrial Technology, Jazan University, Saudi Arabia

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**Abstract**—This document provides a highly detailed and comprehensive review of the recent advancements in hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) sensor technology, bridging the gap between foundational materials science and cutting-edge, real-time diagnostic applications. Hydrogen peroxide is a ubiquitous reactive oxygen species (ROS) that acts as an essential biomarker across clinical diagnostics, food safety, environmental monitoring, and industrial processes. At normal physiological concentrations (1-100 μM), (H<sub>2</sub>O<sub>2</sub>) functions as a critical mediator in cellular signalling pathways, including cell proliferation, immune responses, and apoptosis. However, elevated levels are strongly associated with oxidative stress, which contributes to severe pathological conditions such as cancer, cardiovascular diseases, diabetes, and neurodegenerative disorders. The concentration variations across biological fluids ranging from 1-5 μM in healthy human blood serum, 10-1000 μM in sweat, up to millimolar levels in wound exudate necessitate the development of versatile, highly sensitive, and selective sensor platforms. Traditional detection methods, such as spectrophotometry, chromatography, and chemiluminescence, are limited by their requirement for sophisticated laboratory equipment and time-consuming sample preparation. Consequently, recent innovations in nanotechnology, flexible electronics, and wireless communication have revolutionized this field, driving the transition toward real-time, miniaturized, point-of-care, and continuous monitoring systems.

**Index Terms**—Hydrogen peroxide sensors, electrochemical biosensors, nanomaterials, wearable sensors, optical detection, point-of-care diagnostics

## I. CLASSIFICATION OF H<sub>2</sub>O<sub>2</sub> SENSOR TECHNOLOGIES

The review systematically categorizes (H<sub>2</sub>O<sub>2</sub>) sensors based on their underlying transduction mechanisms, highlighting electrochemical and optical approaches as the predominant methodologies.

### A. Electrochemical Sensors

Electrochemical sensors dominate the field of (H<sub>2</sub>O<sub>2</sub>) detection due to their inherent high sensitivity, exceptionally rapid response times (often under 10 seconds), and compatibility with miniaturization. These sensors are primarily divided into:

**Amperometric Sensors:** Measuring the current generated by the oxidation or reduction of (H<sub>2</sub>O<sub>2</sub>) at a fixed potential, these sensors offer broad linear ranges and profound sensitivity. The fundamental detection mechanism involves electrocatalytic reduction, represented by the chemical reaction: 
$$\text{H}_2\text{O}_2 + 2\text{H}^+ + 2\text{e}^- \rightarrow 2\text{H}_2\text{O}$$
 Advanced nanocomposites enhance their performance. For example, a PtNP/SWCNT/PET sensor achieved a remarkably low limit of detection (LOD) of 228 nM and a dynamic range of 500 nM to 1 M. Similarly, an Au NPs/SnO<sub>2</sub> nanofibers composite exhibited a rapid 6.5-second response and maintained over 90% stability over 41 days.

**Voltametric Sensors:** Utilizing techniques such as cyclic voltammetry (CV), differential pulse voltammetry (DPV), and square wave voltammetry (SWV), these sensors provide critical mechanistic insights into the redox reactions. A notable core-shell Au@TiO<sub>2</sub>/MWCNT sensor utilized this approach to detect (H<sub>2</sub>O<sub>2</sub>) in blood serum and saliva with high selectivity against common interferents like ascorbic acid, uric acid, and glucose.

**Impedimetric Sensors:** These label-free sensors measure changes in electrode impedance upon (H<sub>2</sub>O<sub>2</sub>) binding. While traditionally exhibiting lower sensitivity compared to amperometric methods, the integration of advanced nanomaterial-modified electrodes has significantly enhanced their performance, enabling accurate detection down to the micromolar range.

## B. Optical Sensors

Optical platforms rely on light absorption, emission, or scattering changes upon interaction with (H<sub>2</sub>O<sub>2</sub>).

**Fluorescence-Based Sensors:** Offering supreme sensitivity and multiplexing capabilities, these sensors employ probes like nitrogen-doped carbon quantum dots (N-CQDs). Waste-derived N-doped graphene quantum dots have been developed for both cellular imaging and high-sensitivity (H<sub>2</sub>O<sub>2</sub>) tracking.

**Colorimetric Sensors:** Ideal for instrument-free, visual, point-of-care detection. Developments include portable, intelligent paper-based sensors utilizing horseradish peroxidase (HRP) integrated with smartphone data processing, yielding an LOD of 1.0 µmol/L. Nanozyme-based variations, such as MOF-818, catalyze colorimetric reactions to enable dual-mode visual and electrochemical quantification.

**SERS and SPR Sensors:** Surface-Enhanced Raman Spectroscopy (SERS) provides molecular fingerprinting with single-molecule trace-level sensitivity, while Surface Plasmon Resonance (SPR) enables label-free, real-time monitoring of (H<sub>2</sub>O<sub>2</sub>) interactions by detecting shifts in the refractive index. **Chemiluminescence Sensors:** These platforms monitor light emission from mediated chemical reactions without requiring external light sources, often utilized alongside smartphone cameras for quantitative evaluation.

## II. NANOMATERIAL-ENHANCED SENSOR PLATFORMS

Nanomaterials function as dual-purpose components in modern (H<sub>2</sub>O<sub>2</sub>) sensors serving simultaneously as transducers and catalysts. Their high surface-to-volume ratios, unique electronic attributes, and exceptional electrocatalytic activity are the driving forces behind the next generation of sensing technologies.

**Carbon Nanotubes (CNTs) & Graphene:** CNTs provide exceptional electrical conductivity and mechanical strength. Graphene and its derivatives (such as reduced graphene oxide, rGO) offer robust two-dimensional electron transport networks. Three-dimensional graphene architectures, like a 3D rGO-MXene-MWCNT electrode, facilitate maximum (H<sub>2</sub>O<sub>2</sub>) diffusion to active sites, enabling intraoperative diagnostics for cancer tissue.

**MXenes:** A class of 2D transition metal carbides and nitrides, MXenes (like Ti<sub>3</sub>C<sub>2</sub>) exhibit metallic conductivity and hydrophilicity. When integrated with Nafion and enzymes, they create highly efficient biosensors capable of detecting acute myocardial infarction markers in human serum.

**Metal-Organic Frameworks (MOFs):** MOFs present crystalline, highly porous structures with tunable pore sizes and distinct catalytic active sites. Copper-based 2D/3D MOFs and Au-nanoparticle-embedded UiO-66 MOFs offer stable matrices that prevent nanoparticle aggregation, thereby preserving high long-term catalytic activity.

**Quantum Dots & Metal Nanoparticles:** Transitioning beyond simple carbon structures, sulfur-doped graphene quantum dots, metal nanoparticles (Au, Pt, Ag), and bimetallic single-atom nanozymes (like FeCo systems) fundamentally maximize atomic utilization efficiency, pushing detection limits into the sub-nanomolar realms.

**Metal Oxides:** Architectures such as CuO nanostructures, ZnO nanorods, and multiporous SnO<sub>2</sub> nanofibers facilitate direct electrocatalytic (H<sub>2</sub>O<sub>2</sub>) reduction, providing robust, enzyme-free sensor foundations.

## III. ENZYMATIC VS. NON-ENZYMATIC PARADIGMS

A critical theme in sensor development is the architectural choice between enzymatic and non-enzymatic recognition elements, each presenting distinct trade-offs regarding selectivity, stability, and operational environments.

### A. Enzymatic Sensors

Enzymatic sensors utilize natural biocatalysts, predominantly horseradish peroxidase (HRP), catalase, or bacterial peroxidase.

**Advantages:** Their primary strength lies in exceptional substrate-specific selectivity, which naturally minimizes interference from complex biological matrices. They also benefit from signal amplification provided by biological catalysis and operate seamlessly under mild physiological conditions (pH 6-8, under 40°C).

**Limitations:** Despite their high performance, enzymatic sensors suffer from limited long-term stability due to intrinsic enzyme denaturation. They

are highly sensitive to environmental fluctuations (pH, temperature), require complex immobilization protocols that can alter catalytic activity, are relatively expensive, and face shelf-life constraints.

#### B. Non-Enzymatic Sensors (Nanozymes)

To circumvent the limitations of natural enzymes, the field has aggressively pivoted toward non-enzymatic platforms driven by nanomaterials possessing intrinsic catalytic activity, often termed "nanozymes."

**Advantages:** Nanozymes exhibit extraordinary stability in harsh environments, functioning across broad pH ranges (2-12) and high temperatures (up to 100°C). They boast scalable, low-cost fabrication, wider linear detection ranges (spanning from nanomolar to molar concentrations), and an extended shelf-life lasting months to years.

**Limitations:** The primary drawback is a moderate reduction in selectivity; nanomaterial catalysts often respond to diverse electroactive species. Interference management therefore necessitates strict potential optimization or the application of selective protective membranes.

#### C. Hybrid Approaches

The review emphasizes a modern paradigm shift toward hybrid systems that strategically merge enzymatic specificity with nanozyme durability. For instance, cascade-based wearable biosensors utilize enzymes (like lactate oxidase) for target specificity while relying on highly stable nanozymes to execute the eventual (H<sub>2</sub>O<sub>2</sub>) electrochemical transduction, achieving an optimal balance of selectivity and long-term robustness.

### IV. WEARABLE AND FLEXIBLE SENSOR TECHNOLOGIES

The convergence of flexible electronics with sophisticated biosensing has unlocked continuous, non-invasive health monitoring. Developing these wearable devices requires careful consideration of mechanical flexibility, biocompatibility, and consistent performance under physical deformation (bending, stretching, twisting).

#### A. Diverse Substrates and Structural Design

The foundational substrate significantly dictates the functionality and comfort of wearable sensors:

**Polymer Substrates:** Polyethylene terephthalate (PET) ensures transparency and mechanical stability under bending angles up to 90°. Polydimethylsiloxane (PDMS) provides extreme stretchability, allowing devices to accommodate dynamic body movements without compromising electrical contact. Polyimide (PI) offers superior thermal stability during complex fabrication processes.

**Carbon-Based Substrates:** Carbon cloth establishes a conductive 3D network that eliminates the need for external current collectors. Laser-induced graphene (LIG) polyimide substrates allow for rapid, maskless, cost-effective electrode fabrication.

**Hydrogels & Textiles:** Hydrophilic matrices, such as ferrocene-based hydrogels, mirror the physical properties of biological tissues while facilitating continuous ion transport. Smart textile fabrics and optical core-shell micro fibrous networks integrate sensors directly into everyday clothing or commercial wound bandages.

### V. INNOVATIVE FORM FACTORS

Wearable (H<sub>2</sub>O<sub>2</sub>) sensors have materialized into various highly specialized form factors designed to sample distinct biological fluids:

**Skin Patches:** Screen-printed, biocompatible patches adhere directly to the epidermis, utilizing materials like chitosan and Prussian blue to continuously track reactive oxygen species in human eccrine perspiration over multi-week periods.

**Microneedle Arrays:** Designed to safely penetrate the stratum corneum, these arrays interface with interstitial fluid a matrix that closely mirrors blood composition yielding real-time, second-scale response times without the invasiveness of phlebotomy.

**Smart Contact Lenses:** Long-term stable wireless lenses built with hyaluronate-modified Au@Pt bimetallic electrodes harness tear fluid to provide continuous, digital diagnostic data, particularly valuable for diabetes management.

**Microfluidic Wound Dressings:** Integrated platforms like the "iCares" device continuously analyze wound exudate in situ. They quantify reactive species, allowing clinicians to dynamically assess chronic wound healing status and predict infection risks.

**Implantable Bioresorbable Sensors:** Representing a massive leap in medical hardware, these devices (such as Pt-decorated MoO<sub>3-x</sub> nanozyme sensors)

dynamically monitor deep-tissue inflammation and automatically dissolve within the body once their operational lifespan concludes, eliminating the need for surgical extraction.

Integration of these platforms with custom printed circuit boards (PCBs) and smartphone technology allows for robust, wireless data transmission, transforming passive sensors into active telemedicine diagnostic tools.

## VI. APPLICATIONS ACROSS DIVERSE DOMAINS

The versatility of advanced (H<sub>2</sub>O<sub>2</sub>) sensors enables transformative applications spanning clinical diagnostics, food safety regulations, environmental analysis, and industrial process control.

### A. Clinical Diagnostics and Cell Biology

In the clinical sphere, (H<sub>2</sub>O<sub>2</sub>) detection is heavily leveraged for non-invasive cardiovascular disease monitoring (e.g., detecting biomarkers in acute myocardial infarction patients). Wearable sweat and tear sensors track metabolic and oxidative stress profiles. Furthermore, flexible electrochemical arrays are integrated into direct cell culture setups to monitor in situ cellular (H<sub>2</sub>O<sub>2</sub>) secretion over 72-hour intervals, facilitating breakthrough real-time research in tumour oxidative stress and endothelial Mechanotransduction.

### B. Food Safety and Quality Assurance

Hydrogen peroxide is occasionally utilized illegally as a masking agent for bacterial contamination in dairy. Advanced heterostructure metal oxide sensors integrated onto glassy carbon electrodes precisely estimate (H<sub>2</sub>O<sub>2</sub>) adulteration in complex matrices like raw milk. Additionally, portable paper-based and nanofiber-supported Au nanoparticle sensors successfully evaluate (H<sub>2</sub>O<sub>2</sub>) residues in acidic, high-sugar fruit juices and alcoholic beverages, providing low-cost, on-site food quality assessments.

### C. Environmental Monitoring and Industrial Processes

In ecological contexts, (H<sub>2</sub>O<sub>2</sub>) acts as an imperative indicator of water quality and the oxidative capacity of rainwater. Industrially, carbon hybrid nanocomposite sensors are deployed in municipal wastewater treatment facilities to monitor pollutant degradation

processes in real time. Moreover, they regulate aseptic packaging sterilization protocols, ensuring maximum bacterial eradication while preventing excessive chemical residues that could compromise product integrity.

## VII. CURRENT CHALLENGES AND FUTURE TRAJECTORIES

Despite exponential advancements, the commercialization and clinical translation of next-generation (H<sub>2</sub>O<sub>2</sub>) sensors face several critical bottlenecks that dictate the trajectory of future research.

**Stability and Interference:** Long-term operational stability remains heavily challenged by sensor surface fouling, nanoparticle aggregation, and biomolecular degradation. Mitigation strategies currently involve the implementation of sophisticated protective polymers (e.g., chitosan, Nafion) and periodic regeneration protocols. Additionally, biological fluids introduce severe interference from electroactive species (ascorbic acid, uric acid, dopamine). Enhancing selectivity demands precise applied-potential optimization and the deployment of charge-selective semi-permeable membranes.

**Biocompatibility and Power Solutions:** While carbon-based substrates exhibit excellent biocompatibility, some advanced nanomaterials (like heavy-metal quantum dots) raise critical toxicity concerns requiring careful surface functionalization. Furthermore, powering continuous wearable sensors remains complex; traditional batteries add impractical bulk. The field is rapidly shifting toward self-powered configurations utilizing biofuel cells, solar harvesting, and wireless power transfer.

**Miniaturization and AI Integration:** The future lies in the integration of microfluidics into Lab-on-a-Chip and Organ-on-a-Chip platforms. Artificial Intelligence (AI) and Machine Learning (ML) algorithms will be fundamental in managing the massive data streams generated by continuous sensors, executing real-time signal processing, noise reduction, autonomous drift compensation, and predictive physiological modeling.

**Multiplexing and Closed-Loop Systems:** Future diagnostic platforms will not isolate (H<sub>2</sub>O<sub>2</sub>); they will feature complex arrays detecting multiple ROS species, metabolites, and inflammatory markers simultaneously. The ultimate apex of this technology

is the development of closed-loop therapeutic systems. By bridging continuous ( $H_2O_2$ ) sensing with automated drug delivery (such as ferrocene-based antioxidant hydrogels), future systems will dynamically adjust therapeutic dosages based on real-time biomarker fluctuations, maximizing clinical efficacy.

**Sustainability:** Moving forward, aligning sensor fabrication with "Green Chemistry" principles is paramount. The utilization of waste-derived materials (like N-doped graphene quantum dots), biodegradable electronics, and water-based synthesis protocols will drastically reduce the environmental footprint associated with massive single-use biosensor deployment.

### VIII. CONCLUSION

The evolution of ( $H_2O_2$ ) sensors sit at the intersection of nanotechnology, electrochemistry, and flexible electronics. As research meticulously overcomes current boundaries in selectivity, stability, and biocompatibility, these versatile platforms will cement their role as foundational pillars in the future of personalized medicine, environmental stewardship, and continuous bio-diagnostic monitoring.

Applications of  $H_2O_2$  sensors span clinical diagnostics (cardiovascular disease, cancer, diabetes, wound healing), food safety (milk adulteration, juice quality, beverage monitoring), environmental monitoring (water quality, air quality), and industrial process control (wastewater treatment, aseptic packaging). The versatility of  $H_2O_2$  sensors across these diverse domains underscores their broad impact on human health, food security, and environmental protection.

Despite significant progress, challenges remain in long-term stability, interference management, biocompatibility, calibration, and power supply for wearable sensors. Future research directions include miniaturization and integration, artificial intelligence and machine learning, multiplexed detection, implantable and bioresorbable sensors, closed-loop therapeutic systems, advanced nanomaterials, standardization and regulatory approval, and sustainability considerations.

The convergence of nanotechnology, materials science, flexible electronics, and wireless communication is driving  $H_2O_2$  sensor technology toward a future of personalized medicine, continuous

health monitoring, and point-of-care diagnostics. As these technologies mature and overcome current limitations,  $H_2O_2$  sensors will play an increasingly important role in improving human health, ensuring food safety, and protecting the environment.

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